

Introduction

Hydroxyapatite [HAp] clearly has a great potential for biomedical applications because of its similarity in chemical composition and crystalline structure to human hard tissue [1,2]. However, relatively poor strength and fracture toughness have restricted its extensive applications. A great deal of work has been done on the research and development of HAp ceramics as biomaterials [3-7]. One possible solution for improving the mechanical properties is microwave sintering of HAp [8-11].

Microwave sintering of HAp has been studied by Fang et al. [12-14]

Experimental Procedure

Raw materials

Four commercially available pre-calcined HAp powders, including P81, P88, P120 and P149 (Plasma Biotol Ltd., Tideswell, Derbyshire, England), were used. BM16 powder was prepared by bead milling P149 HAp powder, with sixteen passes. Table 1 shows the average particle size and specific surface area of the HAp powders used in this work. For sintering studies, the powders were uniaxially pressed into pellets of 12.7 mm diameter.

Microwave hybrid heating: A 1.5 kW, 2.45 GHz variable-power microwave furnace (Ceramic Engineering, Sydney, Australia), with proportional power control (amplitude variation) and built-in mode stirrer, was used at the 65% power level for all experiments.

HAp is only weakly microwave-absorbent at low temperatures. It therefore cannot be heated from room temperature without a susceptor. However, like most ceramics, its microwave absorption capability increases with temperature [28]. Therefore, a microwave hybrid heating procedure was required to heat the HAp samples from room temperature to the critical temperature T_{crit} above which HAp can efficiently absorb microwave radiation.

A cylindrical clay-bonded silicon carbide susceptor ($\phi=60$ mm, $h=20$ mm) was positioned around the sample. The susceptor was placed inside an alumina brick (120×280 mm), which was surrounded by a layer ($240 \times 240 \times 200$ mm) of fibrous aluminosilicate insulation (Kaowool, Morganite Industrial Products, Sydney, Australia). This arrangement is shown schematically in Figure 1. For each experimental run, one sample was placed at the centre of the susceptor. The temperature was measured with an infrared pyrometer, which was calibrated during the cool-down cycle using a Pt - Pt13Rh thermocouple. A standard heating rate of $\sim 10,000^\circ\text{C}/\text{h}$ and a soak time of 10 min were used. The mode stirrer was used at all times to produce a more uniform microwave field distribution across the cavity.

Conventional heating: An electric furnace ($300 \times 200 \times 120$ mm) with SiC elements (Gallenkamp, London, UK) was used for the conventional heating of the control samples. A standard heating rate of $300^\circ\text{C}/\text{h}$ (the furnace maximum) and soak time of 60 min were used in all cases. No serious overshooting was observed by such a high heating rate. Two sets of experimental trials were carried out.

Comparative densification and decomposition behaviour: Pellets from each of the HAp powders were sintered at a range of temperatures, from 900°C to 1400°C in 100°C steps by microwave and conventional heating. After sintering, the apparent density and %HAp yield of the pellets were measured according to the methods described by Ruys et al. [29].

Effect of microwave soak time: To investigate the effect of microwave soak time, one pellet from each powder was microwave sintered at 1100°C using soak times of 1, 3, 10 and 30 min. No conventionally sintered controls were used in this study. After sintering, the apparent density of the pellets was measured to determine the effects of microwave soak time on the densification behaviour of HAp ceramics.

Results and Discussion

Comparative densification behaviour

Figures 2-6 present the sintering curves of the HAp powders

sintered by microwave and conventional heating. They reveal that, with microwave sintering, densification began at $\sim 900^\circ\text{C}$ - 1000°C , which was $\sim 100^\circ\text{C}$ - 150°C lower than for conventional sintering. These data show that the maximum densities were achieved at $\sim 1200^\circ\text{C}$ - 1400°C (the sintering plateau temperature for microwave heating) for microwave heating as compared with $\sim 1300^\circ\text{C}$ - 1400°C (the sintering plateau temperature for conventional heating) for conventional heating. In other words, microwave heating below the conventional heating plateau temperature significantly improved densification. However, the densities obtained above the conventional heating plateau temperature were similar for microwave or conventional heating.

The densities attained after sintering at 1100°C using microwave and conventional sintering are shown in Figure 7. These data show

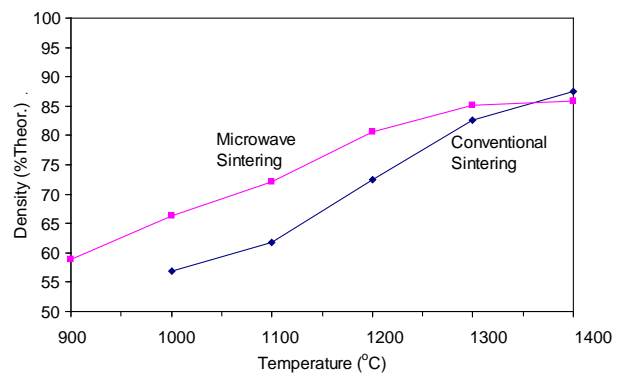


Figure 2: Comparative sintering curves for P81 HAp sintered by microwave and conventional heating.

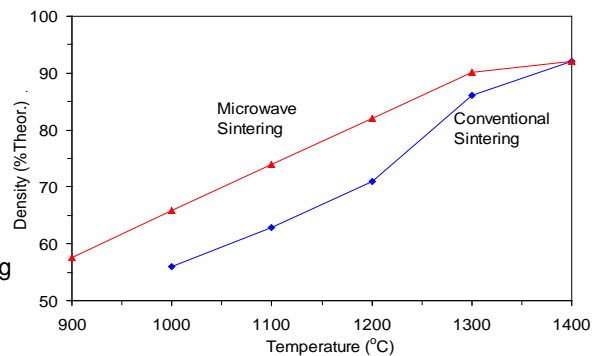
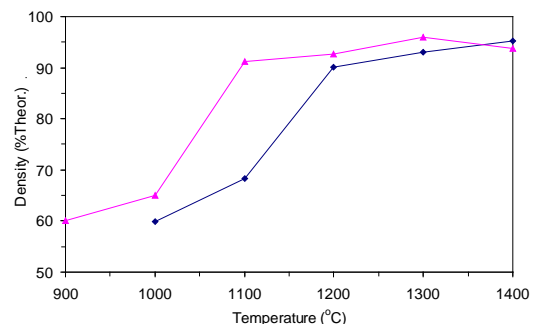


Figure 3: Comparative sintering curves for P88 HAp sintered by microwave and conventional heating.



that microwave heating significantly improved densification for each of the powders trialled. Overall, the improvement in densification by microwave heating at 1100°C was of the order of ~11-30%. Although the soaking time for the microwave and conventionally processed samples are different, the comparison is valid below the composition temperature, where no decomposition occurs. At higher temperature, however, using identical soaking times would be more reliable.

Therefore the main difference between microwave and conventional heating in this trial was the fact that densification occurred at lower temperatures for the former. This is advantageous in the case of HAp since lower sintering temperatures reduce the risk of decomposition.

Therefore, it appears that microwave sintering offers a solution to the problem of trying to achieve maximal densification of HAp without the

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was crystalline while the structure of the surface was amorphous. The existence of an amorphous layer on the surface of the microwave sintered grains suggests the presence of a liquid phase at the particle surfaces during microwave sintering. This would enhance densification.

It has also been suggested that, in microwave sintering, the temperature between particles is higher than the apparent or measured temperature and the supposed formation temperature of the liquid phase [55]. This temperature heterogeneity will decrease the liquid viscosity in the grain boundaries. Moreover, the vibration rate and amplitude of the liquid molecules will be increased by preferential coupling of the microwaves with the liquid formed in the grain boundaries. This also will reduce the liquid viscosity. The presence of a liquid with low viscosity increases the rate of grain rearrangement, thereby enhancing the densification rate.

This theory has been confirmed by Tiegs et al. [56-59], who have shown that preferential coupling of microwaves with the grain boundaries in microwave heated Si_3N_4 -based ceramics leads to improved densification. Ferber et al. [60] established that the improved creep resistance of microwave-heated $\text{Ni}_3\text{Si}_2\text{O}_3\text{-2Al}_2\text{O}_3$ was due to the preferential coupling of microwave radiation with the intergranular phases. It has been suggested that relatively small temperature gradients across the grains can induce a driving force to encourage densification [54].

Figures 3-7 shows that the temperature for the onset of densification for either microwave or conventional heating was lower for the powders with smaller particle size and higher surface area (such as BM16 and P120). The sintering characteristics of a powder depend on the surface area, particle size, particle size distribution, morphology and reactivity [61]. For a given chemical reactivity, densification at a given temperature will be enhanced with a finer particle size, higher surface area, and appropriate size distribution for dense particle packing. The temperature at which the maximum density was achieved also depended on the particle size and surface area of the powders. In case of BM16 impurities also have possibly affected the density. It was lower for the powders with a smaller particle size and higher surface area.

Figure 7 shows that the densification enhancement of microwave heating was strongly dependent on the particle size of the powders. The densification enhancement for the finer HAp powders, such as BM16 and P120, was much greater than that for the coarser HAp powders, such as P81, P88 and P149. Compared with conventional sintering, microwave sintering of the powder (BM16) at 1100°C led to a ~30% (64.5% versus 94.5% dense) densification enhancement whereas, it led to only a 5% increase in decomposition (76% versus 81%). The fact that densification is enhanced much more than decomposition is a positive result, which points to practical benefits in processing of reinforced HAp biomaterials. The reason for this strong enhancement of densification (compared with a weak enhancement of decomposition) is that the decomposition rate during microwave heating was probably increased by the induced higher diffusion rate, whereas densification was enhanced by both the induced higher diffusion rate and the preferential grain boundary coupling mechanism. Therefore, any disadvantage in decomposition should be partially compensated by advantages in densification.

Effect of microwave soak time: A number of combinations of powder type and soak time were trialled at a soak temperature of 1100°C. The results are shown in Figure 8. These data indicate that, for three pure HAp powders (P88, P120 and P149), increasing soak times led to a slight improvement in densification level, although little improvement occurred for soak times above 3 to 10 min. Therefore, a 3 min soak time is sufficient for HAp powders required for bone replacement.

Sample	Conventional Sintering (%)	Microwave Sintering (%)	Soak Time (min)
BM16	64.5	94.5	3, 10
P81	76	81	3, 10
P88	76	81	3, 10
P120	76	81	3, 10
P149	76	81	3, 10

